

# Identifying Microwave Antenna Design Limitations for Radar-based Breast Imaging

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**Abstract**—Clinical trials using ten different Microwave Breast Imaging systems have been published including both academic and industrial systems. While trials with over 200 participants show promising detection results, substantial technical differences exist between the systems in terms of the antenna designs, antenna array designs and antenna performance specifications. In this work, the current state-of-the-art in operational microwave systems in terms of antennas are reviewed and preliminary limits on dimensions are identified. Gaps in understanding regarding the optimal number, configuration and performance of antennas are highlighted and future work regarding the impact of these design decisions on imaging performance identified.

**Index Terms**—microwave breast imaging; microwave imaging; propagation

## I. Introduction

In the last five years alone, clinical trials of microwave breast imaging systems from more than seven operational systems have been published with both academic and industrial interest of which many reviews exist, not least [1]–[4]. While many consistent and promising trends are evident in terms of the potential to detect early-stage or otherwise difficult to detect cancers, many technical differences exist between the systems [2].

Specifically, differences exist in terms of the numbers of antennas in the system, the antenna positions and ability or necessity of antennas to move, how the full microwave scan of the breast is acquired and in the design of the antennas themselves. Few studies have examined the optimal antenna parameters in terms of antenna dimensions, type or performance in terms of required bandwidth, frequency range or adaptability, although preliminary work suggests that antenna layout and orientation can affect performance [5].

Many open-source and shared resources are available for microwave breast imaging research, including:

- numerical breast phantoms [6];
- shared 3-d printed breast phantoms and experimental datasets [7]–[9];
- and open-source imaging toolboxes [1], [9], [10].

However, no open-source antenna designs, shared antenna resources or electromagnetic simulation platforms exist for the acquisition of data.

In this work, basic design parameters for antennas for microwave breast imaging systems are reviewed and identified, specifically, preliminary limitations on the antenna dimensions required to cover a microwave breast imaging radome. Finally, other uses of similar non-invasive biomedical microwave imaging systems are reviewed.

## II. Existing Implementations

Many antenna types have been used in operational systems, not least:

- monopole antennas in [11];
- cavity-backed slot antennas [12].
- Vivaldi antennas [13], [14];
- planar slot antennas [15];
- horn antennas [16];
- and flexible microstrip antennas [17].

These antennas have been incorporated into flexible wearable arrays, rigid fixed housing, moveable subarrays or moveable antennas. The frequency ranges of use have varied from 0.5 GHz to 9 GHz with bandwidths as small as 2 GHz in [17] to much larger in [13].

Antennas have been designed which operate entirely in air [9], directly in contact with the breast [15], [17], in contact with a solid coupling shell [12], in contact with an immersion

tank [14], and immersed in a tank of varying fluids [11], [13].

While some work has considered the optimal frequency ranges in terms of penetration [18], investigations of inherent assumptions in [19], comparisons using different patient orientations in [20] and some other analyses not least in [1], [3], no comprehensive guidelines on minimum performance standards of antenna arrays for microwave breast imaging have been established.

### III. Design Goals

Broadly speaking, the antenna array should be able to:

- illuminate the object of interest from multiple aspects;
- sample the scattered field from multiple aspects;
- and couple sufficient energy into the object of interest.

The majority of microwave breast imaging antennas operate either in air, in direct contact with a coupling shell or tank, or immersed in a tank of coupling liquid. The coupling liquids or coupling shells are typically designed to secure the breast, to match the dielectric properties of the skin ( $\epsilon_r \approx 30$ ), or to provide a consistent operating environment.

To estimate the necessary maximum dimensions to ensure a minimum number of antennas, a simplified model of an acquisition surface is examined consisting of a hemisphere of radius  $R$ , similar to MARIA [12] and other systems comprehensively reviewed in [2]. Typically in these systems, the antennas  $\mathbf{a}_i \in \mathcal{A}$  are arranged in concentric rings of decreasing radius  $R_n$  in the coronal plane, meaning the maximum number of antennas can be calculated as:

$$|\mathcal{A}| = \sum_n^N \left\lfloor \frac{\pi}{\arctan(w/2R_n)} \right\rfloor \quad (1)$$

where the number of coronal rings,  $N$  can be calculated:

$$N = \left\lfloor \frac{\pi/4}{\arctan(h/2R)} \right\rfloor \quad (2)$$

and the radius of each ring is:

$$R_n = R \cos n\theta \quad (3)$$

For a square antenna where  $w = h$ , the maximum number of antennas for hemispheres between with radii between 6 to 9 cm is shown in Figure 1 with the 60 antennas of the MARIA

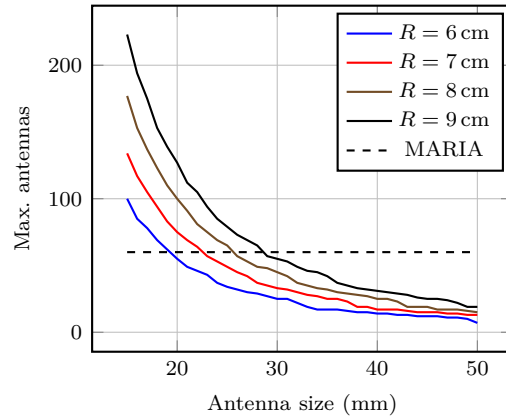


Fig. 1. The maximum number of square antennas which could form a conformal hemispherical antenna array for radomes of four different radii are shown. For reference, the number of antennas in the MARIA system in [12] are also shown.

system shown for reference. As can be seen, even for large arrays of 9 cm in radius, the total antenna assembly including supports and separators must be less than  $3 \text{ cm} \times 3 \text{ cm}$  to fit greater than 60 antennas in the hemisphere.

For antennas with differing widths and heights, few studies have examined if an optimal antenna arrangement exists or what the minimum number of acceptable antennas is. For example, narrower but tall antennas allow for more antennas in the coronal rings at the expense of fewer rings which may be desirable. In some cases such as in [11], [14], data is collected in successive coronal slices, meaning that the antenna width alone determines the number of antennas in the array.

Further discretisations of the acquisition surface are possible and some studies suggest that non-regular or randomised arrays might improve performance [21]. Enhanced understanding of the effects of antenna positioning on performance may refine the understanding.

Directivity of the antennas also varies, from omnidirectional monopoles in the tomographic system in [11] to more directive antennas in the other radar-based systems. However, few studies have examined the desirable characteristics in terms of directivity. Limits on the directivity based on minimum power levels within the imaging volume are calculated in [22].

### IV. Related Applications

Active microwave systems are also used in other applications, not least:

- non-invasive systems for monitoring or treatment;
- endobronchial systems for treatment;
- and percutaneous systems for treatment.

Focusing solely on external, non-invasive systems, many cross-overs exist. For example, active microwave hyperthermia systems are in use which couple focused microwave energy into the head and neck to raise the temperature of shallow tumours as part of a treatment regime [23]. Typically the antennas are submerged in a water bolus [24] and often consist of a single ring of antennas for shallow tumour treatment.

Active microwave systems have also been investigated for hydration monitoring [25], [26] using easily accessible limbs and also for bone health monitoring using joints such as the ankle [27]. However, in these applications, three dimensional images or imaging arrays are not required. While microwave breast imaging of the head has been proposed, few similarities exist between these applications due to the hair, desired targets and the presence of the skull.

#### V. Conclusion

As microwave breast imaging is used with larger and more diverse populations, it may be necessary to identify performance specifications and key design decisions to ensure adequate and consistent imaging performance. However, substantial gaps in the literature remain regarding many aspects of the antenna array design specifically in the optimal size, arrangement and performance characteristics of the antennas. In this work, preliminary size limitations on the antennas are identified, however, further examinations of how the arrangement and sizes of the antennas might impact on the imaging performance is warranted.

#### References

- [1] N. K. Nikolova, Ed., *Introduction to Microwave Imaging*, ser. EuMA High Frequency Technologies Series. Cambridge, UK: Cambridge University Press, Jul. 2017.
- [2] D. O’Loughlin, M. O’Halloran, B. M. Moloney, et al., “Microwave Breast Imaging: Clinical Advances and Remaining Challenges,” *Transactions on Biomedical Engineering*, vol. 65, no. 11, pp. 2580–2590, Nov. 2018.
- [3] J.-C. Bolomey, “Crossed Viewpoints on Microwave-Based Imaging for Medical Diagnosis: From Genesis to Earliest Clinical Outcomes,” en, in *The World of Applied Electromagnetics*, A. Lakhtakia and C. M. Furse, Eds., Cham, Switzerland: Springer International Publishing, 2018, pp. 369–414.
- [4] B. M. Moloney, D. O’Loughlin, S. Abd Elwahab, et al., “Breast cancer detection: A synopsis of conventional modalities and the potential role of microwave imaging,” *Diagnostics*, vol. 10, no. 2, Feb. 2020, Art. 103.
- [5] D. Kurrant, J. Bourqui, C. Curtis, et al., “Evaluation of 3-D Acquisition Surfaces for Radar-Based Microwave Breast Imaging,” *IEEE Transactions on Antennas and Propagation*, vol. 63, no. 11, pp. 4910–4920, Nov. 2015.
- [6] M. J. Burfeindt, T. J. Colgan, R. O. Mays, et al., “MRI-Derived 3-D-Printed Breast Phantom for Microwave Breast Imaging Validation,” *IEEE Antennas and Wireless Propagation Letters*, vol. 11, pp. 1610–1613, 2012.
- [7] N. Joachimowicz, B. Duchêne, C. Conessa, et al., “Easy-to-produce adjustable realistic breast phantoms for microwave imaging,” in *Proceedings of the 10th European Conference on Antennas and Propagation (EuCAP)*, Davos, Switzerland: IEEE, Apr. 2016, pp. 1–4.
- [8] B. L. Oliveira, D. O’Loughlin, M. O’Halloran, et al., “Microwave Breast Imaging: Experimental tumour phantoms for the evaluation of new breast cancer diagnosis systems,” *Biomedical Physics & Engineering Express*, vol. 4, no. 2, Feb. 2018, Art. 025036.
- [9] T. Reimer, J. Krenkevich, and S. Pistorius, “An open-access experimental dataset for breast microwave imaging,” in *14th EuCAP*, Copenhagen, Denmark: IEEE, Mar. 2020.
- [10] D. O’Loughlin, M. A. Elahi, E. Porter, et al., “Open-source software for microwave radar-based image reconstruction,” in *Proceedings of the 12th European Conference on Antennas and Propagation (EuCAP)*, London, the UK: IEEE, Apr. 2018.
- [11] P. M. Meaney, M. W. Fanning, T. Reynolds, et al., “Initial Clinical Ex-

- perience with Microwave Breast Imaging in Women with Normal Mammography,” *Academic Radiology*, vol. 14, no. 2, pp. 207–218, Feb. 2007.
- [12] A. W. Preece, I. J. Craddock, M. Shere, et al., “MARIA M4: Clinical evaluation of a prototype ultrawideband radar scanner for breast cancer detection,” *Journal of Medical Imaging*, vol. 3, no. 3, p. 033502, Jul. 2016.
- [13] E. C. Fear, J. Bourqui, C. F. Curtis, et al., “Microwave Breast Imaging With a Monostatic Radar-Based System: A Study of Application to Patients,” *IEEE Transactions on Microwave Theory and Techniques*, vol. 61, no. 5, pp. 2119–2128, May 2013.
- [14] A. Fasoula, L. Duchesne, J. Gil Cano, et al., “On-Site Validation of a Microwave Breast Imaging System, before First Patient Study,” en, *Diagnostics*, vol. 8, no. 3, p. 53, Aug. 2018.
- [15] H. Song, S. Sasada, T. Kadoya, et al., “Detectability of Breast Tumor by a Hand-held Impulse-Radar Detector: Performance Evaluation and Pilot Clinical Study,” en, *Scientific Reports*, vol. 7, no. 1, Dec. 2017, Art. 16353.
- [16] F. Yang, L. Sun, Z. Hu, et al., “A large-scale clinical trial of radar-based microwave breast imaging for Asian women: Phase I,” in *Proceedings of the International Symposium on Antennas and Propagation (APSURSI)*, San Diego, CA, USA: IEEE, Jul. 2017, pp. 781–783.
- [17] E. Porter, M. Coates, and M. Popović, “An Early Clinical Study of Time-Domain Microwave Radar for Breast Health Monitoring,” *IEEE Transactions on Biomedical Engineering*, vol. 63, no. 3, pp. 530–539, Mar. 2016.
- [18] J. Lin, “Frequency optimization for microwave imaging of biological tissues,” *Proceedings of the IEEE*, vol. 73, no. 2, pp. 374–375, 1985.
- [19] C. F. Curtis, B. R. Lavoie, and E. C. Fear, “An Analysis of the Assumptions Inherent to Near-Field Beamforming for Biomedical Applications,” *IEEE Transactions on Computational Imaging*, vol. 3, no. 4, pp. 953–965, Dec. 2017.
- [20] D. Wörtge, J. Moll, V. Krozer, et al., “Comparison of X-ray Mammography and Planar UWB Microwave Imaging of the Breast: First Results from a Patient Study,” en, *Diagnostics*, vol. 8, no. 3, Aug. 2018, Art. 54.
- [21] K. Nemez, A. Baran, M. Asefi, et al., “Modeling Error and Calibration Techniques for a Faceted Metallic Chamber for Magnetic Field Microwave Imaging,” *IEEE Transactions on Microwave Theory and Techniques*, vol. 65, no. 11, pp. 4347–4356, Nov. 2017.
- [22] H. Benchakroun, A. Fasoula, L. Duchesne, et al., “Coverage estimation for microwave imaging using full multi-static radar imaging algorithms with restricted opening,” in *Proceedings of the 14th European Conference on Antennas and Propagation (EuCAP)*, Copenhagen, Denmark: IEEE, Mar. 2020.
- [23] N. R. Datta, S. Rogers, S. G. Ordóñez, et al., “Hyperthermia and radiotherapy in the management of head and neck cancers: A systematic review and meta-analysis,” *International Journal of Hyperthermia*, vol. 32, no. 1, pp. 31–40, 2016, PMID: 26928474. eprint: <https://doi.org/10.3109/02656736.2015.1099746>.
- [24] M. M. Paulides, J. F. Bakker, E. Neufeld, et al., “The hypercollar: A novel applicator for hyperthermia in the head and neck,” *International Journal of Hyperthermia*, vol. 23, no. 7, pp. 567–576, 2007. eprint: <https://doi.org/10.1080/02656730701670478>.
- [25] D. C. Garrett and E. C. Fear, “Feasibility study of hydration monitoring using microwaves—part 1: A model of microwave property changes with dehydration,” *IEEE Journal of Electromagnetics, RF and Microwaves in Medicine and Biology*, vol. 3, no. 4, pp. 292–299, 2019.
- [26] B. C. Besler and E. C. Fear, “Microwave hydration monitoring: System assessment using fasting volunteers,” *Sensors*, vol. 21, no. 21, 2021.
- [27] P. M. Meaney, D. Goodwin, A. H. Golnabi, et al., “Clinical microwave tomographic imaging of the calcaneus: A first-in-human case study of two subjects,” *IEEE Transactions on Biomedical Engineering*, vol. 59, no. 12, pp. 3304–3313, 2012.